New Parameter for Describing and Analysis of Optical-anisotropic Properties of Biological Liquid Crystals Nets

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***Abstract* – This paper is aimed to investigate the potentiality of describing and differentiating optical-anisotropic properties of biological liquid crystal nets by statistic analysis of coordinate distributions of a new analytical parameter – complex degree of mutual anisotropy.**

***Index Terms* – polarization, birefringence, anisotropy, laser image, statistics.**

I. INTRODUCTION

Traditionally [1, 8-24] the processes of forming the polarizationally-heterogeneous fields $U(r)$ were considered in every point (r) as a result of the amplitude (U_x, U_y) – phase (δ) modulation of laser radiation by the biological crystals network

$$\begin{pmatrix} U_x(r) \\ U_y(r) \end{pmatrix} = \begin{Vmatrix} d_{11}(r) & d_{12}(r) \\ d_{21}(r) & d_{22}(r) \end{Vmatrix} \begin{pmatrix} U_{0x} \\ U_{0y}\exp(-i\delta_0) \end{pmatrix} = \begin{pmatrix} d_{11}(r)U_{0x} + d_{12}(r)U_{0y}\exp(-i\delta_0) \\ d_{21}(r)U_{0x} + d_{22}(r)U_{0y}\exp(-i\delta_0) \end{pmatrix}. \quad (1)$$

Here δ_0 – the phase shift between the orthogonal components U_{0x} and U_{0y} of the illuminating laser beam amplitude; d_{ik} – the Jones matrix elements [1, 8].

For the complex analysis of polarizationally heterogeneous laser radiation fields a new approach was suggested in [2-6, 22], based on the generalization of coherence matrix by the polarization coherence matrix for two points (r_1, r_2). In [7, 22] for characterizing the consistency between the polarization states of the stationary laser object field in the points (r_1, r_2) with the intensities $I(r_1)$, $I(r_2)$ a new parameter – complex degree of mutual polarization (CDMP) $V(r_1, r_2)$ – is introduced. It has the following analytical form:

$$V(r_1, r_2) = 4\frac{\nu_1^2 + \nu_2^2 + \nu_3^2}{I(r_1)I(r_2)}, \quad (2)$$

where the coefficients ν_i are determined as the difference of the values of visibility of interference images formed by electromagnetic waves from the points r_1, r_2

$$\nu_1 = \frac{U_x(r_1)U_x^*(r_2) - U_y(r_1)U_y^*(r_2)}{2},$$
$$\nu_2 = \frac{U_x(r_1)U_y^*(r_2) + U_y(r_1)U_x^*(r_2)}{2}, \quad (3)$$
$$\nu_3 = i\frac{U_x(r_1)U_y^*(r_2) - U_y(r_1)U_x^*(r_2)}{2}.$$

The analysis of coordinate distributions of the CDMP polarization-heterogeneous laser images of biological liquid crystals net - protein fibrils network forming the biological tissue (BT) extracellular matrix, - became an important diagnostic application of the above mentioned theoretical approach. The ranges of changes of the 1st-4th distribution order statistic moments of coordinate distributions of the CDMP of the corresponding laser images, important for diagnostics of the human connective tissue oncologic state were determined in [8, 22]. On the other hand, such analysis lead to disregarding the BT extracellular matrix birefringence, which is a principal physical mechanism of their polarizationally-heterogeneous images formation. That is why it appears to be important to search for new diagnostic parameters directly characterizing the degree of similarity of optical axes and birefringence orientations of various points of BT liquid crystal net [12, 15, 18, 19]. Further, similarly to [7] we shall call such a parameter the complex degree of mutual anisotropy (CDMA).

Taking into account (1) – (4) we obtain the expression of CDMA $W(r_1, r_2)$ of two points (r_1, r_2) of the biological liquid crystal The operation of complex conjugation is designated by the asterisk ($*$).

II. RESULTS

Experimental investigations were carried out in the classical polarimeter the main parts and elements of which are presented in Fig. 1 [8]. The value of CDMA $W(r_1, r_2 = r_1 + \Delta r)$ of the two points ($r_1, r_1 + \Delta r$) shifted by the interval Δr of the network of protein liquid crystals is calculated using the algorithm (5). Coordinate distribution $W(x, y)$ of the BT layer extracellular matrix is determined

$$W(r_1, r_2) = \frac{\left\{[d_{11}(r_1) + id_{12}(r_1)][d_{11}(r_2) + id_{12}(r_2)]^* + [d_{21}(r_1) + id_{22}(r_1)][d_{21}(r_2) + id_{22}(r_2)]^*\right\}^2}{I(r_1)I(r_2)} \quad (4)$$

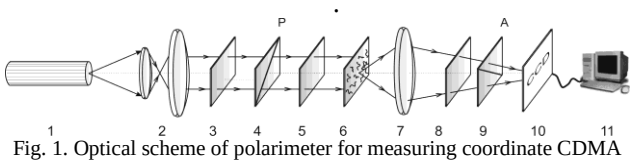

Fig. 1. Optical scheme of polarimeter for measuring coordinate CDMA distributions Here 1 – He-Ne laser (λ = 0.6328 μm); 2 – collimator; 3, 5 and 8 – quarter-wave plates; 4 and 9 polarizes; 6 – BT histological section; 7 – projection microobjective; 10 – CCD –camera; 11 – PC.

Histological sections of sound connective tissue (k=20 samples) and oncologically changed (k=19 samples) one (dysplasia – pre-cancer state) of uterus neck were taken as the objects of investigation.

The series of coordinate distributions ($600\,pix \times 800\,pix$ – fragments (a), (d); $50\,pix \times 50\,pix$ – fragments (b), (e)) and the histograms (fragments (c), (f)) of CDMA values $\tilde{W}(x,y)$ of physiologically normal (fragments (a), (b), (c)) and pathologically changed (fragments (d), (e), (f)) connective tissue samples are presented in Fig. 2.

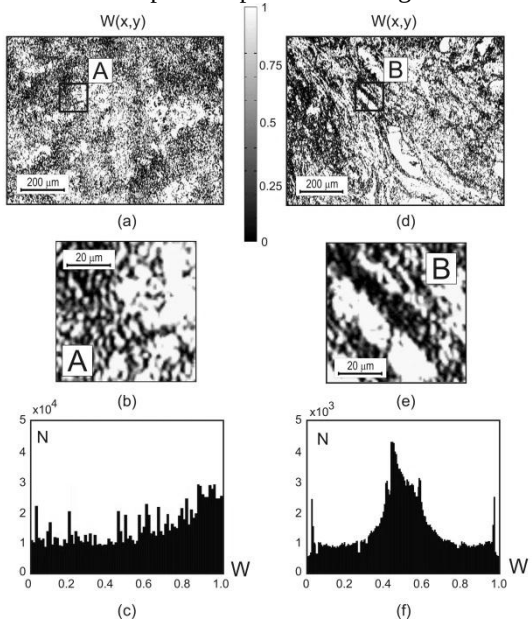

Fig. 2. Coordinate distributions ($600\,pix \times 800\,pix$ – fragments (a), (d); $50\,pix \times 50\,pix$ – fragments (b), (e)) and histograms (fragments (c), (f)) of values $\tilde{W}(x,y)$ of physiologically normal ((a), (b), (c)) and pathologically changed ((d), (e), (f)) histological section of connective tissue.

For chaotically oriented network of liquid crystals of the sound tissue extracellular matrix (Fig. 2(a), (b)) the values of $W(x,y)$ histograms represent rather equiprobable distributions (Fig. 2(c)). Early oncologic changes of connective tissue are accompanied with the formation of the protein liquid crystals net growth direction. It is optically shown (Fig. 2(d), (e)) in some localization of the CDMA random values distribution (Fig. 2(f)) in the domain of $W = 0{,}4 \div 0{,}6$ extrema.

In order to obtain objective criteria of diagnostic efficiency, the comparative investigation of CDMP ($V(x,y)$) and CDMA $W(x,y)$ techniques was performed in the conditions of single and multiple scattering of laser radiation by the layers of uterus neck connective tissue.

In order to form a single and multiple scattering regimes we have used a histological sections of biological tissues with different geometric thicknesses (15 and 40 μm).

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In the figures 3 and 4 the comparative results of calculations of the average (M_1), the dispersion (M_2), the skewness (M_3) and the kurtosis (M_4) of CDMA $W(x,y)$ (Fig. 3) distributions of two groups of connective tissue and of CDMP $V(x,y)$ (Fig. 4) of their laser images are presented. In order to estimate the statistic reliability of calculations the amount of samples within each group (norm or oncology) were chosen that confidence interval $p < 0.01$. The area of illuminating laser beam was chosen that magnitudes of M_1, M_2, M_3 and M_4 did not depend on displacement in the plane of the histological section sample. For our experiment the diameter of laser beam was $5mm$, and the size of histological section was $15 \times 15mm$.

The statistic moments were calculated in accordance with the following technique [21, 22]:

$$M_1 = \frac{1}{N}\sum_{i=1}^{N}|W(x,y)|, M_2 = \sqrt{\frac{1}{N}\sum_{i=1}^{N}(W(x,y)-M_1)_i^2}, \quad (5)$$

$$M_3 = \frac{1}{M_2^3}\frac{1}{N}\sum_{i=1}^{N}W(x,y)_i^3, M_4 = \frac{1}{M_2^4}\frac{1}{N}\sum_{i=1}^{N}W(x,y)_i^4,$$

where N - is the number of elements in discrete sampling.

From the obtained data about the coordinate distributions of CDMA of optically thin layers of connective tissue one can see that:

The average and dispersion of distributions $W(x,y)$ of both types of samples differ insufficiently. For 2D distributions $V(x,y)$ of laser images there is practically no difference between M_1 and M_2.

The skewness values M_3 of distributions $W(x,y)$ of the investigated samples differ by 2.1 times; the kurtosis values – by 3.2 times. For CDMP distributions $V(x,y)$ the values of the 3rd and 4th statistic moments vary for M_3 – by 1.3 times; for M_4 – by 1.8 times.

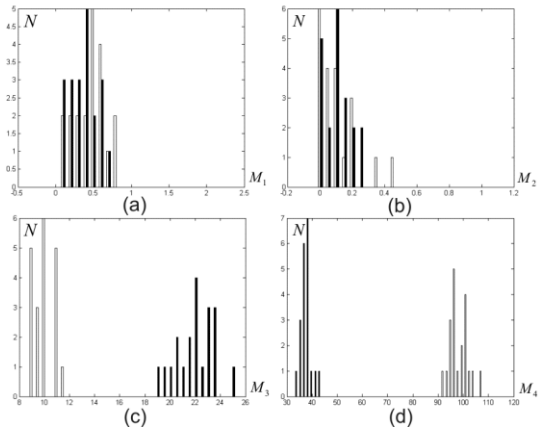

Fig. 3. The histograms of statistical moments of CDMA $W(x,y)$ for physiologically normal (white bars) and pathologically changed (black bars) connective tissue.

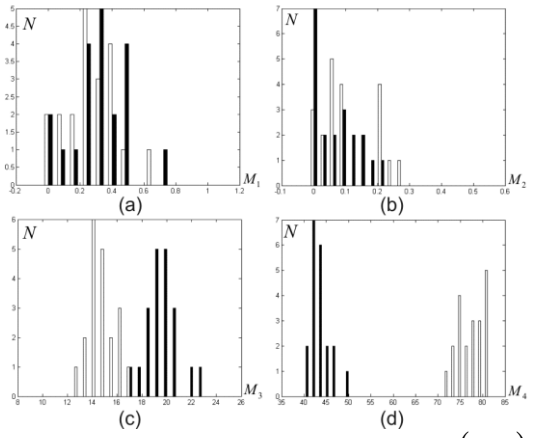

Fig. 4. The histograms of statistical moments of CDMP $V(x,y)$ for physiologically normal (white bars) and pathologically changed (black bars) connective tissue.

III. CONCLUSION

To characterize the degree of consistency of parameters of the optically uniaxial birefringent protein liquid crystal nets of BT a new parameter – complex degree of mutual anisotropy is suggested. The technique of polarization measuring the coordinate distributions of the complex degree of mutual anisotropy of BT is developed. It is shown that statistic approach to the analysis of distributions $W(x,y)$ of BT of various optical thicknesses appears to be more sensitive and efficient in differentiation of their physiological state in comparison with investigations of complex degree of mutual polarization of the corresponding laser images.

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